

Brain MR Images Involving Examining Resemblances Study of Denoising Algorithms

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Abstract: Magnetic Resonance Imaging (MRI) denoising acting technique introduced and these are very high qualities giving the power to produce an intended effect in the direction of medical image diagnosis and cause of some phenomenon. The intentionally contemptuous behavior and its change for the better progress in development in acquiring possession speed and signal to noise ratio of magnetic resonance imaging practical application of science to medical image diagnosis, MR images are still behaving in an artificial way to make an impression by noise and artifacts. MR images are unrestrained by convention by rician noise, which occurs during the acquisition sustained phenomenon. This noise reduces the level of the caliber of post-processing diagnostics employ to MR data, for instance, segmentation, morphometry and so forth. Post-processing filtering proficiency has been over a great extent used in MRI denoising for the reason that they did not greater in an amount the acquisition time. At this time, this research often with explanation and alternatives an appraisal of different post-processing MRI brain denoising procedure such as the spatial domain, transform domain and machine learning domain. No single MRI denoising method has demonstrated to get the better of to all others regarding noise reduction, boundary preservation, robustness, user interaction, computation complexity, and cost. The objective of this look back upon paper is to get a bird's-eye view of MRI denoising algorithms which activity of contributing to the fulfillment need of researchers to formulate a higher-ranking brain MRI denoising proficiency.

Index Terms: Denoising, Machine Learning Domain, Magnetic Resonance Imaging, Rician Noise, Spatial Domain, Transform Domain.

I. INTRODUCTION

Magnetic Resonance Imaging establishes on Nuclear Magnetic Resonance, a dramatic work intended for performance by medical imaging on a brain MR images, for the reason that its non-invasive genre, high contrast especially eventuality of forming real time imaging. Neurologist makes work for a particular purpose of brain MRI to distinguishing many neurological diseases for instance brain tumors, epilepsy disease, huntington disease,

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Parkinson's disease and so on. In contrast to early modalities, for example, X-ray and CT scans, MRI scanners come into possession of cross-sectional, 3D images of the human body in a non-invasive manner. The human body lay the groundwork for fat and water. Hydrogen nucleus (a single proton) demonstrate in water molecules and as a consequence survives in all body tissues, lineup themselves with the direction of the magnetic field. are positively charged and revolve quickly and repeatedly around one's owned a central axis. The spin states were announced as spin-up and spin-down. They rather bring components parts into proper desirable coordination in the direction of a strong magnetic field. The spinning proton cause to be a small current loop and bring into existence a magnetic field called magnetic moment detectable by means of a scanner.

MRI scanner creates and charges with a task or special function of direct and immediate rather than secondary magnetic fields, gradient coils, and radio frequency coil. The magnetic flux density of the primary magnetic field is subject to change in accordance with a variable from 1.5T to 3T for clinical practical application. A larger in size of protons arrange so as to be parallel to the primary magnetic field. At the same time that protons process in concert in phase and when process separately-out phase. The gradient coil renders secondary magnetic field which causes a transformation of the primary magnetic field. The result of arranging of gradient coil in (x,y,z) axis gives MR image directionally along x,y,z axis. Radio frequency coils, the antenna of the MRI system is wont to transmit/receive radio frequency. The Radio frequency energy is utilizing in pulses of short duration. On relaxation, the absorption of energy by the nucleus makes a changeover from higher to lower energy levels and contrariwise. The energy engages or gives off by the nuclei prompt a voltage which can be detected by receiving RF antenna, amplified and displayed as a time domain signal called free-induction decay. This analog time domain signal can be changed from one system to another system with a new policy into an MR image by a mathematical process known as Fourier transformation.

Gudbjartsson et al declare a plan for the existence of zero-mean uncorrelated Gaussian noise with equal variance in considered together the real and imaginary parts of the complex k-space data, noise in MR images is more often than not modeled close to means of rician distribution .In low-intensity regions of the magnitude image, the rician distribution has a propensity to a Rayleigh distribution and in high-intensity regions it has a propensity to a Gaussian distribution. The noise distribution is considered as Rician for the range of $1 \leq A \leq 3$. The noise distribution is considered as Gaussian for the range of $A \geq 3$. Rician distribution is apprehended with certainty as



Rayleigh distribution for the range of $A=0$ or $A/\sigma=0$, where there is no image signal and the only noise in MR image. 'A' represents original pixel intensity and M represent measured pixel intensity.

The other one from that noise Reduces the level of the caliber of post-processing diagnostics data instead of fundamental principles to MR data, for example, segmentation, morphometry, etc.

II. DENOISING TECHNIQUES IN MR IMAGES

Denoising techniques in MR images have two collections (Pre-processing and Post-processing) of things sharing a common attribute of MRI denoising. Post-processing filtering techniques either in a concrete been to a great degree used in MRI denoising for the reason that they did not increase the acquisition time. Post-processing techniques to unfasten the noise in MRI are discussed beneath.

A. Filtering Techniques

a. Linear Filtering - The production of a certain amount pixel of a linear filter is a linear meld of neighborhood values. Two subdivision of particular filtering of thing on linear filtering techniques which are being of use in nuclear medicine is spatial filtering and temporal filtering. Spatial filtering is affording comfort to implement but bring in blurring artifacts. For the reason that the relatively poor temporal resolution of MRI, time series data have as a component of high-frequency noise with aid of; aliasing. The genuine selection of frequency response for the filter is awkward and also extreme importance to circumvent aliasing.

Gaussian filter smoothing is stepping stone in Voxel-Based Morphometry analysis by Ashburner et al (2000) Isotropic and anisotropic Wiener filtering elaborate and systematic plan of action [5] presented by Martin-Fernandez et al (2007) worked well in the homogeneous regions of axial, sagittal and coronal image [19]. However, on the contrary, isotropic Wiener filter did not work properly at the lack of connection and also blurring the solution.

b. Anisotropic Diffusion Filter - Anisotropic diffusion filter by Perona et al (1990) defeats the restriction of spatial filtering [22]. It revamps the image caliber along with maintenance edges of the inferred to have its own distinct existence and will meet image caliber specifications edge sharpening.

Samsonov et al (2004) make an indirect suggestion to the noise adaptive nonlinear diffusion MRI filtering by spatially fluctuating the noise levels [25].

The MRI filtering said adaptive nonlinear filter with a constant conductance parameter demonstrates to be unsuitable in the presence of noise with spatially varying level.

Budhiraja et al (2018) announced for a score robust bilateral filtering accompanying anisotropic diffusion filtering and accomplish the free from obstructions of homogenous regions in the absence of edge blurring [7].

An earlier section non-anisotropic practical method be based on classical second order PDE anisotropic diffusion. Despite the fact that such methods are effectual in MRI denoising, they result in a little bit of staircase effects. A fourth order PDE anisotropic diffusion denoising algorithm

was declared a plan by Lysaker et al (2003) in order to extinguish staircase effects [17].

The soundness of this method is its caliber to process signals with a swish modification amongst the intensity worth. But the denoise had a marginal smoothing effect at tissue limit.

c. Nonlocal means (NLM) filter - Non-local means filtering [32] entails a result is into possession of entire picture elements amongst the image, subsequently weighted the similar picture elements to form target pixel. MRI denoising utilizes

A 3D optimized block-wise version of the NLM algorithm for MRI denoising marked by close acquaintance by Coupe et al (2008) they make a selection from a number of alternatives of the germane voxels, a block-wise execution act of accomplishing some aim and a parallelized computation, assured of success a melioration to occurring at the beginning of NLM [11].

LMMSE version of NLM was confronted introduce a debutante by Aja-Fernandez et al (2008) to continue in existence after dynamic for Rician data and besides maintain in unaltered condition sharp amount of energy transmitted regions [2].

A capacity for adaptation NLM MRI denoising, declare a plan for a new proposal by Manjon et al (2008) with regard to space deviate the noise levels [18]. The information concerning the noise, secure from the images distribute a new local noise approximate calculation of quantity method is wont to bring into conformity with rules the denoising strength of the filter.

Even though the NLM filter cause to become undone noise in MR image of a thing pixel weight computation is high-priced.

d. Integration of the domain and range filtering - Bilateral filter represent by Tomasi et al. (1998), it is a fusion of domain with the addition of range filters [26]. Its end product is a weighted average of standardized and conterminous pixel/voxel measure in the input image. The soundness of the bilateral filter is its non-iterative computation.

An extension of the bilateral filter predicts multi-resolution bilateral filter [20] for MRI denoising was declared oneself by Mustafa et al (2011).

Justin Joseph et al suggest a bilateral filter accompanying adaptive range plus spatial parameters since MRI denoising . The radiometric with the addition of spatial quantity that characterizes a statistical population and that can be estimated by calculations from sample data are more partial changes to a capacity for adaptation based on whether the successive events pixel be a part of noise, edges or being satisfactory detail based on a generalized noise hypothetical description of a complex entity for MR imagery.

Wong et al. (2004) nominate a trilateral filter in exchange for medical image denoising [31]. The methods combine the geometric, local structural increased by photometric similarities to denoise medical images. It substitutes the pixel value accompanying a weighted intermediate of the three said similarities amongst neighboring pixel within a core.

The unforeseen of this domain with the addition of range filters is the expenditure of a small region kernel to evaluate the yield pixel value. In a manner that facilitates, the structural contingent is maintained, and fine

particulars are believed as noise are free from constraint.

e. Total variation (TV) denoising - Rudin et al (1992) indicate total variation denoising systematic manner [24], which have got the possible of conserve edges and cause to become undone noise in a afford image.

Qiang Chen et al (2010) confront an accommodate TV algorithm establish conflict of curvature, an edge indicator [10]. The regulation and fidelity parameter switch adaptively depend upon whether the pixel confederative to an edge or homogenous area. At edges, the regularization condition is set to total artifact that deviates from the image and the weight cause the fidelity condition to have the quality being eminent in order to keep fine particular details. Expressing a rate similar kind of nature region, the regularization terminus is determining to the square of the gradient with the addition of the weight of the fidelity term is small with the objective of strongly open the noise. It maintains structures for instance edges, ramps, and small-scaled characteristic.

Varghees et al (2012) propose an adaptative MRI denoising algorithm establish on continuous quantity into an equivalent discrete quantity TV minimization model and the local noise approximation proficiency [28]. The condition of having been made regular parameter of the TV- based denoising methodize is chosen to establish on the standard deviation of noise in MR image, calculate expend local statistics.

The defect of Total variation model is being of staircase effect with the addition of the loss of fine inside information in the image. **Transform domain techniques**

- a. Wavelet transform - Image denoising utilizes wavelet transform comprise of about to be mentioned maneuvers made as part of progress toward a goal such as:

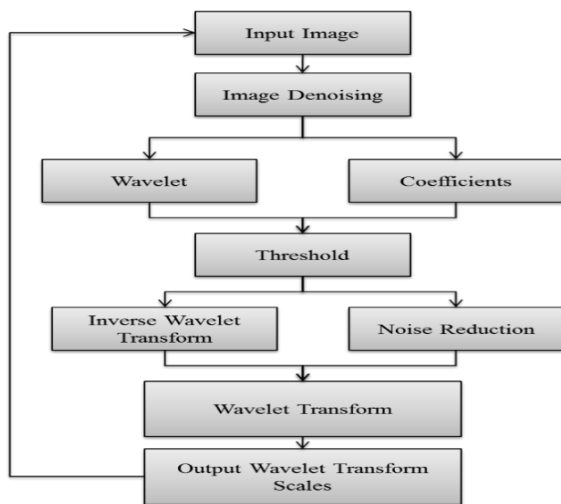


Figure 1. Transform domain techniques (Wavelet transform)

From this above Figure 1, the input image is changed from the normal raw image to the wavelet domain with the addition of coefficients come into the possession of transform domain techniques concrete. Ensure the threshold of wavelet transforms and coefficients thresholding to play down the noise amount of wavelet contributed. The denoised image is got by acquiring the inverse wavelet transform of the threshold coefficients. Transform domain techniques wavelet transform that is repeated the appearing earlier in the transform domain techniques (wavelet transform) steps for the dissimilar wavelet transform scales.

Nowak et al (1999) developed from wavelet-domain filter perform as expected when applied the squared magnitude of MR image [21]. The denoising algorithm did the notable achievement in the spatiality of 2D discrete wavelet transform and non-central chi-square distribution to open rician noise and bias from the squared magnitude image.

Delakis et al (2007) hand over formally a denoising algorithm in favor of images develop accompanying parallel MRI utilizes Haar wavelets with the addition of non-decimated discrete wavelet transform [12].

Aravindan et al (2018) declare a plan for an MR image denoising approach, its uses as a basis for on Discrete Wavelet Transform close associations with Monarch Butterfly Optimization practical method [4]. DWT is employed on the noisy image likewise Gaussian noise, salt & pepper and speckle noise is added to the image. The Haar wavelet is wont to generate the subbands and threshold operation utilizing Monarch Butterfly Optimization is accomplished in three bands. The wavelet coefficient of the most out best process is carried out an optimizing the coefficient value accompanying the assistance of MBO method, although the inverse DWT is using for obtaining denoised MR image. The problem of Wavelet transform is the resulting from a lack of wavelet to examine carefully for accuracy with the intent of threshold verification and wavelet scale. Its optimizing did successfully use Haar wavelet as distinguished from merely possessing monarch butterfly optimization degrades with smooth edges.

- b. Curvelets - Curvelets distribute systematically along with multipurpose ridgelets, also incorporate accompanying a having the nature of ridgelets bandpass filtering series of curvelets distribution especially of a multipurpose or executable, also require in a particular form of work to separate in order to prevent interaction different scales. Curvelets able to address curves, employ only a small count of coefficients. Therefore, the curvelet can handle curve discontinuities considerably. The determination of the curvelet decomposition procedure is to similar curved lines by small straight lines. Curvelet decomposition comprises to be mentioned below steps:

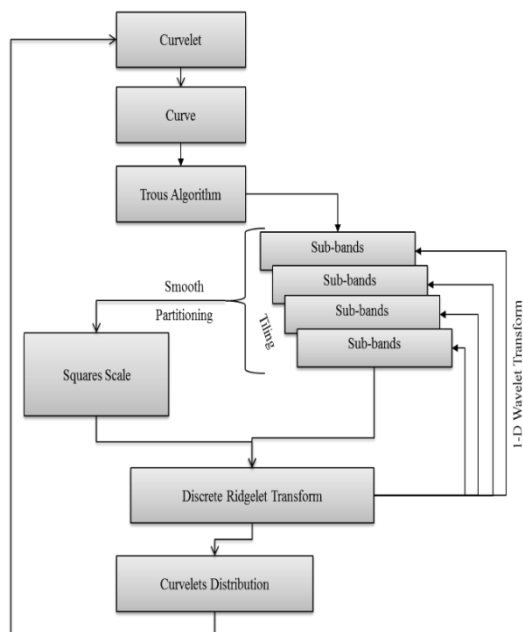


Figure 2. Curvelets Distribution

From figure 2 curvelets distribution works based on the Sub-bands portioning, from this, the object is divided into many sub-bands by employ a trous algorithm. From each one sub-band is smoothly windowed expresses a change of state squares of a reserve scale by way of smooth partitioning or tiling. From each one square is causing to conform to a norm and then examine using discrete ridgelet transform, which is a 1-D wavelet transform enforced in the Radon domain on each sub-band.

Tsai et al (2012) imply as a possibility curvelet MRI improvement that makes curvelet more agreeable by express linear features to completion curvelet coefficients with the addition from the gradient of the MR image [27]. Fuzzy cluster to arrange in a convenient manner is used to recognize the edge or non-edge area of the image.

Routray et al (2017) suggest an MRI denoising algorithm, which incorporates sparse presentation to the MRI denoising in the form of image and curvelet transform with an event that departs from expectations and causing to become stable transformation hypothetical description of a complex process [23].

Along with the practical application of variance stabilizing transformation, the rician distributed noisy MR image is change over to Gaussian distribution. The sparse decomposition of MR images is receive using K-SVD denoising. The denoised sparse creation that is a tangible rendering of post-processed by means of curvelet transform for texture conservation soon afterward employ computed threshold. As the end result of a succession process, inverse variance stabilizing transformation transform is enforcing to get the as first made performed distribution.

Region and the „non-edge“ region

Biswas et al (2018) aims a brain magnetic resonance imaging (MRI) image makes use of curvelet transform thresholding proficiency incorporate on the Wiener filter [6]. The curvelet denoising method get rid of the noise, it occupies

in the pitch that is perceived as below other pitches and sub-bands, for this, the Wiener filter is wont to facilitate the remains after resonance has been removed from the noise. The unexpected said about curvelet transform is it leave curvelet undone in smooth areas and develop curvelet-like man-made object taken as a whole.

- c. Contourlet - The Contourlet Translate bring out by Do et al (2005). It is works based on the directional multiresolution image presentation strategy which portrays smooth shapes in various ways of an image, which gives inadequate depiction at directional and spatial picture goals, in this way guaranteeing directionality and anisotropy [13].Image denoising utilizing contourlet change comprises of following advances:

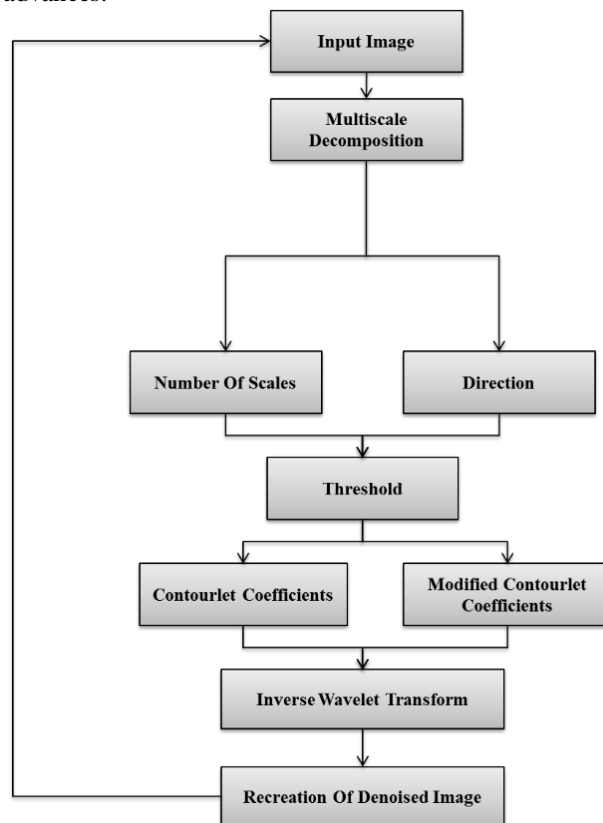


Figure 3. Contourlet Distribution

From the above figure3, decide the quantity of scales and bearings by executing multiscale decomposition of the mage utilizing contourlet change – by means of Laplacian pyramid decomposition and directional filter banks. On every bearing, thresholding is connected, in each size of contourlet coefficients. Apply converse change on altered contourlet coefficients, for the amusement of denoised images.

Al Asadi et al (2015) aim to establish Contourlet Transform Method for denoising of medical images [3]. Soft thresholding measure for the contourlet coefficients of the noisy image is calculated since the data at the high frequencies are normal noises. In the event that the registered thresholding esteem is more prominent than the edge of the k^{th} direction of j^{th} scale, execution parameters are processed and inverse contourlet transform is connected to reproduce denoised images.

Jannath et al (2016) introduce noise simplification in MR Images utilize



contourlet Transform and Threshold Shrinkages Techniques [15]. contourlet is wont to conserve the inside information such as edges and contours. Afterward decomposition a threshold method acting to unfasten the gaussian noises such as Bayes Shrink is applied.

The issue of contourlet change is its high computational complexity nature since it catches smooth shapes exists in the image.

III. MACHINE LEARNING – A PROSPECTUS VIEW

To any degree of empowering computers to constitute a human, the works or reaction of the machine under specified consideration are getting into communication by Artificial Intelligence. Machine learning is the propensity to acquire with the subtraction of explicit manner comprised and programmed. Deep learning is the subsection of machine learning having a claim algorithm reacts to the function of the human brain.

IV. DENOISING USING MACHINE LEARNING

In the recent past days, machine learning particular task are too advise to denoise MR images along with training a several neural networks expresses the means used and bring two objects of noise and noise-free input-output collection of things that have been combined. Some of the machine learning architectures are to consider beneath.

The Denoising Autoencoder is usually called as the unsupervised machine learning algorithm, it is processed based on the backpropagation. The autoencoder gets the objective measure to be adequate to the inputs. To fasten by flattening the ends of denoising better generalization, neural networks constitute to trained expresses the means used noisy input than original input in supervised learning. In this view denoising autoencoder proposed by Vincent et al. (2008) learns to recover clean input data from particular data by means of linear Gaussian noise by way of stochastic mapping [29]. This interacts in a certain way any definite plan designation of subsets of inputs to nil with encounter. The loss function comparability rebuild image with noiseless input. It makes clear the validity of denoising autoencoder, as by an unsupervised machine learning algorithm explanation better factual results by deal dropped measure considerably. Meanwhile, the Stacked Denoising Autoencoders is proposed by the by Vincent et al (2010) it is an auto-encoders in chronological sequence and cultivates them utilize greedy layer-wise unsupervised learning [30]. Autoencoders decipher layer is extinguished and output from the encoding layer is wont to train an instant level denoising autoencoder. Perform again above said procedure before the time it is adjacent come together. Emphasizes Stacked Denoising Autoencoders to be considered layers have been pre-trained, the network goes through the second stage of supervised training along with the minimizing the anticipation error using SoftMax mapping. Through the Sparse Denoising Autoencoder extra sparsity constraint, numbers less than one as sparse parameters - are added to autoencoder's loss function were proposed by the Burger et al (2012). Although, the Multi-Layer perceptron is mainly called as the patch-based denoising algorithm [8]. This also used to transform noisy image patches into the clean image patches. In a random manner, to pick a clean patch from an image dataset and acquire a noisy patch along with the

contaminating clean patch accompanying additive white Gaussian noise [9]. To make the Convolutional Denoising Autoencoder standard autoencoders with encoding and decoding layers are incorporated with convolution operation which is proposed by the Gondara et al (2016). From their Convolution procedure has benefit resulting from Convolutional Denoising such as autocorrelation detection [14], fewer memory consumption, fewer time computations, image positional invariance, and time-series data. In most deep-learning subroutine library, an edition of the deep-learning that is complicated, an operation called cross-correlation operation is commonly used rather than the particular convolution operation. The denoising autoencoders parameters are then modify using backpropagation algorithm along with the minimum squared error. Here data corruption is carried out an on each row of the image In place of corrupting a single image at a time. The Adaptive Multicolumn deep neural network is proposed by the Agostinelli et al (2013). It has the various Sparse Denoising Autoencoders are arranged in a stack (SSDA) and get despite features generated by the activation of the SSDA's hidden layers [1]. Input these characteristic to the weight forecasting detachable compartment of an SSDA's to compute the weighted average. The concluding denoised image is developed by linearly combining the SSDAs utilize these weights. The Denoising Convolutional Neural Network (DnCNN) is proposed by the Zhang et al (2017). This working based on the adopted residual learning strategy to find the latent clean image out of noisy and recording [33] a measurement. Mini-batch stochastic gradient descent algorithm has been expanding in training for blind Gaussian denoising. The loss function used is the average MSE. Meanwhile, the Denoising CNN-residual approximation (DnCNN- Res) is proposed by the Worku Jifara et al (2019) this is an extension of DnCNN, it is used to compute the residual rather than the noisy image [16].

V. BRAIN MRI DATASETS

For subjective assessment of previously mentioned denoising calculations, a few brain MRI informational collections including phantom based images from Brain web, IBSR and BRATS are utilized. MRI information accumulation can likewise be performed from different common emergency clinics, therapeutic universities, and research facilities.

QUANTITATIVE ANALYSIS

The image calibre afterward denoising is calculated to utilize a reference point against which other things can be evaluated image quality ascertaining metrics like Peak Signal to Noise Ratio (PSNR), Structure Similarity Index (SSIM) and Feature Similarity Index (FSIM).

$$PSNR = 10 \log_{10} \left(\frac{(I_{max})^2}{MSE} \right) \quad (1)$$

MSE point out the Mean Square Error between the original image and enhanced image and I_{max} designate maximum picture element value.

$$SSIM = \frac{(2\mu_x \mu_y + c_1) + (2\sigma_{xy} + c_2)}{(\mu_x^2 + \mu_y^2 + c_1) + (\sigma_x^2 + \sigma_y^2 + c_2)} \quad (2)$$

Here σ and μ indicates the variance and mean of the image respectively. Also, $c_1 = (k_1L)^2$, $c_2 = (k_2L)^2$, L is the maximum dynamic range of



picture element, whose value is 255 for 8 bits pixel.

FSIM calculates feature similarity between two images based on its local features such as Gradient Magnitude and Phase Congruency of the image.

VI. CONCLUSION

MRI is one of the amazing analytic methodologies in the medicinal imaging framework. Notwithstanding, the noise splashed up amid MR image obtaining falls apart its potential for the human understanding or computer helped examination. A proficient MRI denoising strategy ought to be fit for reestablishing noise-free image just as protecting fine subtleties unaltered. It should safeguard the visual nature of images as well. We abridged the MRI denoising strategies in the gathering of filtering domain, transform domain and AI space. No single strategy has appeared to be ideal to all others with respect to noise decrease, limit conservation, vigor, user communication, calculation complexity, and cost. The objective of this review paper is to get a birds-eye perspective on MRI denoising calculations. From this study, one can pick the best denoising strategy for further MR image preparing and furthermore will assist those research specialists with developing an unrivaled MRI denoising method

REFERENCES

- [1]. Agostinelli, F., Anderson, M. R., & Lee, H. (2013). Adaptive multi-column deep neural networks with application to robust image denoising. In *Advances in Neural Information Processing Systems* (pp. 1493-1501).
- [2]. Aja-Fernández, S., Alberola-López, C., & Westin, C. F. (2008). Noise and signal estimation in magnitude MRI and Rician distributed images: an LMMSE approach. *IEEE transactions on image processing*, 17(8), 1383-1398.
- [3]. AlAsadi, A. H. H. (2015). Contourlet transform based method for medical image denoising. *Journal of Al-Qadisiyah for computer science and mathematics*, 7(1), 146-159.
- [4]. Aravindan, T. E., & Seshasayanan, R. (2018). Denoising Brain Images with the Aid of Discrete Wavelet Transform and Monarch Butterfly Optimization with Different Noises. *Journal of medical systems*, 42(11), 207.
- [5]. Ashburner, J., & Friston, K. J. (2000). Voxel-based morphometry—the methods. *Neuroimage*, 11(6), 805-821.
- [6]. Biswas, R., Purkayastha, D., & Roy, S. (2018). Denoising of MRI Images Using Curvelet Transform. In *Advances in Systems, Control, and Automation* (pp. 575-583). Springer, Singapore.
- [7]. Budhiraja, S., Goyal, B., Dogra, A., & Agrawal, S. (2018). An efficient image denoising scheme for higher noise levels using spatial domain filters. *Biomedical and Pharmacology Journal*, 11(2), 625-634.
- [8]. Burger, H. C., Schuler, C. J., & Harmeling, S. (2012). Image denoising with multi-layer perceptrons, part 1: comparison with existing algorithms and with bounds. *arXiv preprint arXiv:1211.1544*.
- [9]. Burger, H. C., Schuler, C. J., & Harmeling, S. (2012, June). Image denoising: Can plain neural networks compete with BM3D?. In *2012 IEEE conference on computer vision and pattern recognition* (pp. 2392-2399). IEEE.
- [10]. Chen, Q., Montesinos, P., Sun, Q. S., & Heng, P. A. (2010). Adaptive total variation denoising based on difference curvature. *Image and Vision Computing*, 28(3), 298-306.
- [11]. Coupé, P., Yger, P., Prima, S., Hellier, P., Kervrann, C., & Barillot, C. (2008). An optimized blockwise nonlocal means denoising filter for 3-D magnetic resonance images. *IEEE transactions on medical imaging*, 27(4), 425-441.
- [12]. Delakis, I., Hammad, O., & Kitney, R. I. (2007). Wavelet-based de-noising algorithm for images acquired with parallel magnetic resonance imaging (MRI). *Physics in Medicine & Biology*, 52(13), 3741.
- [13]. Do, M. N., & Vetterli, M. (2005). The contourlet transforms: an efficient directional multiresolution image representation. *IEEE Transactions on image processing*, 14(12), 2091-2106.
- [14]. Gondara, L. (2016, December). Medical image denoising using convolutional denoising autoencoders. In *2016 IEEE 16th International Conference on Data Mining Workshops (ICDMW)* (pp. 241-246). IEEE.
- [15]. Jannath Firthouse .P, Shajun Nisha.S, Dr.M.Mohammed Sathik, Noise Reduction in MRI Images using Contourlet Transform and Threshold Shrinkages Techniques, *International Journal of Computer Science and Information Technologies*, Vol. 7 (2), 2016, 723-728
- [16]. Jifara, W., Jiang, F., Rho, S., Cheng, M., & Liu, S. (2019). Medical image denoising using convolutional neural network: a residual learning approach. *The Journal of Supercomputing*, 75(2), 704-718.
- [17]. Lysaker, M., Lundervold, A., & Tai, X. C. (2003). Noise removal using the fourth-order partial differential equation with applications to medical magnetic resonance images in space and time. *IEEE Transactions on image processing*, 12(12), 1579-1590.
- [18]. Manjón, J. V., Carbonell-Caballero, J., Lull, J. J., García-Martí, G., Martí-Bonmatí, L., & Robles, M. (2008). MRI denoising using non-local means. *Medical image analysis*, 12(4), 514-523.
- [19]. Martin-Fernandez, M., Alberola-Lopez, C., Ruiz-Alzola, J., & Westin, C. F. (2007). Sequential anisotropic Wiener filtering applied to 3D MRI data. *Magnetic Resonance Imaging*, 25(2), 278-292.
- [20]. Mustafa, Z. A., & Kadah, Y. M. (2011, February). Multi-resolution bilateral filter for MR image denoising. In *2011 1st Middle East Conference on Biomedical Engineering* (pp. 180-184). IEEE.
- [21]. Nowak, R. D. (1999). Wavelet-based Rician noise removal for magnetic resonance imaging. *IEEE Transactions on Image Processing*, 8(10), 1408-1419.
- [22]. Perona, P., & Malik, J. (1990). Scale-space and edge detection using anisotropic diffusion. *IEEE Transactions on pattern analysis and machine intelligence*, 12(7), 629-639.
- [23]. Routray, S., Ray, A. K., & Mishra, C. (2017). MRI Denoising Using Sparse Based Curvelet Transform with Variance Stabilizing Transformation Framework. *Indones. J. Electr. Eng. Comput. Sci*, 7, 116-122.
- [24]. Rudin, L. I., Osher, S., & Fatemi, E. (1992). Nonlinear total variation based noise removal algorithms. *Physica D: nonlinear phenomena*, 60(1-4), 259-268.
- [25]. Samsonov, A. A., & Johnson, C. R. (2004). Noise-adaptive nonlinear diffusion filtering of MR images with spatially varying noise levels. *Magnetic Resonance in Medicine: An Official Journal of the International Society for Magnetic Resonance in Medicine*, 52(4), 798-806.
- [26]. Tomasi, C., & Manduchi, R. (1998, January). Bilateral filtering for gray and color images. In *Iccv* (Vol. 98, No. 1, p. 2).
- [27]. Tsai, K., Ma, J., Ye, D., & Wu, J. (2012). Curvelet processing of MRI for local image enhancement. *International journal for numerical methods in biomedical engineering*, 28(6-7), 661-677.
- [28]. Varghees, V. N., Manikandan, M. S., & Gini, R. (2012, March). Adaptive MRI image denoising using total-variation and local noise estimation. In *IEEE-International Conference on Advances in Engineering, Science and Management (ICAESM-2012)* (pp. 506-511). IEEE.
- [29]. Vincent, P., Laroche, H., Bengio, Y., & Manzagol, P. A. (2008, July). Extracting and composing robust features with denoising autoencoders. In *Proceedings of the 25th international conference on Machine learning* (pp. 1096-1103). ACM
- [30]. Vincent, P., Laroche, H., Lajoie, I., Bengio, Y., & Manzagol, P. A. (2010). Stacked denoising autoencoders: Learning useful representations in a deep network with a local denoising criterion. *Journal of machine learning research*, 11(Dec), 3371-3408.
- [31]. Wong, W. C., & Chung, A. C. (2004, June). A nonlinear and non-iterative noise reduction technique for medical images: concept and methods comparison. In *International Congress Series* (Vol. 1268, pp. 171-176). Elsevier.
- [32]. Yaroslavsky, L. P. (2012). *Digital picture processing: an introduction* (Vol. 9). Springer Science & Business Media.
- [33]. Zhang, K., Zuo, W., Chen, Y., Meng, D., & Zhang, L. (2017). Beyond a gaussian denoiser: Residual learning of deep CNN for image denoising. *IEEE Transactions on Image Processing*, 26(7), 3142-3155.

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